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Potential of Transcranial Direct Current Stimulation in Alzheimer's Disease: Optimizing Trials Toward Clinical Use

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Transcranial direct current stimulation (tDCS) is a safe and well-tolerated noninvasive method for stimulating the brain that is rapidly developing into a treatment method for various neurological and psychiatric conditions. In particular, there is growing evidence of a therapeutic role for tDCS in ameliorating or delaying the cognitive decline in Alzheimer's disease (AD). We provide a brief overview of the current development and application status of tDCS as a nonpharmacological therapeutic method for AD and mild cognitive impairment (MCI), summarize the levels of evidence, and identify the improvements needed for clinical applications. We also suggest future directions for large-scale controlled clinical trials of tDCS in AD and MCI, and emphasize the necessity of identifying the mechanistic targets to facilitate clinical applications.

Keywords transcranial direct current stimulation; Alzheimer disease; clinical trial.

INTRODUCTION

Alzheimer's disease (AD) represents a major global health challenge whose prevalence is increasing along with the aging population. There is an urgent need for effective treatment options for the 24 million people currently living with AD. Unfortunately, despite intensive drug development and research, AD remains without a cure, and current treatment options offer inadequate benefit in delaying its progression. While we await a cure for AD, our near-term approach is to improve its care by preserving functioning and delaying decline.

Noninvasive brain stimulation is rapidly developing as a nondrug treatment for use in a wide range of neurological and psychiatric conditions.² One extensively investigated technique is transcranial direct current stimulation (tDCS), which involves delivering a low-intensity sustained electrical current to cortical tissue via scalp electrodes with the goal of modulating brain excitability and plasticity.3 Based on the cumulative effects of tDCS, a period of repeated sessions (e.g., daily) can be used to induce alterations in brain function that will have clinical effects.4-6

simultaneous rehabilitative activities (e.g., cognitive, motor, or psychotherapeutic). Directing tDCS at a brain region activated during training can enhance the potency of that training, presumably based on the mechanisms via which tDCS can boost ongoing plasticity.9-12 Since tDCS devices can be wearable and portable, they offer the further advantage of providing treatment to patients at home and in other locations away from the clinic through telehealth. 13,14 In this manner, patients can access tDCS treatment away from the clinic and thereby receive the necessary number of daily repeated applications over time so as to maximize its clinical benefit.

tDCS is a safe and well-tolerated treatment approach^{7,8} that can be easily combined with

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There is growing evidence of a therapeutic role for tDCS in ameliorating or delaying the cognitive decline in AD. As reviewed in detail elsewhere, 6,15 clinical trials have found tDCS to be safe and tolerable for use in the AD population, with therapeutic benefits of preserving or even improving cognitive functioning in the short term. However, clinical applications of tDCS remains restricted by the need for definitive clinical trials and the identification of the mechanisms underlying its beneficial effects. Here we focus on optimizing the design of large-scale controlled clinical trials and identifying the mechanistic targets to facilitate clinical applications of tDCS.

OVERVIEW OF tDCS

tDCS is a noninvasive brain stimulation technique that involves passing a low-amplitude direct current (typically 1–2 mA) through the brain via electrodes on the scalp (Fig. 1). The placement locations of the electrodes are determined based on the targeted brain region. A portion of the applied current that crosses the brain leads to polarization of neurons, 16 which in turn modulates excitability, synaptic efficacy, 17 oscillations, 18 plasticity, 19,20 and other cellular processes that are key to cognitive function and learning. 21 The electrode polarity (anode or cathode) determines the direction of current flow, which influences the outcomes. 8,22

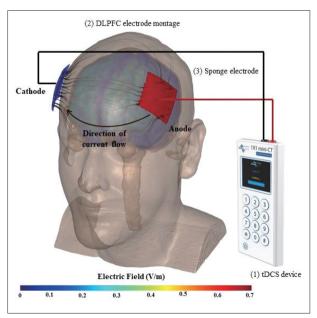


Fig. 1. Transcranial direct current stimulation (tDCS) equipment, working principle, and modeling of the electric field distribution. (1) tDCS device: programmable session type (active or sham), stimulation duration, and current intensity. (2) Dorsolateral prefrontal cortex (DLP-FC) electrode montage (left to right, F3-F4 according to the international 10-20 system). (3) Sponge electrodes.

Based on hundreds of clinical trials in patients with a wide range of neurological and psychiatric conditions, including studies of patients with mild cognitive impairment (MCI) and AD, tDCS has an extensive record of safety and tolerability. 7,23,24 Its advantages over other stimulation methods such as transcranial magnetic stimulation (TMS) include easier use, lower cost, and better tolerability (e.g., not associated with seizures^{25,26}). As also reported previously, the mostcommon side effects involve transient sensations at the electrode site and include tingling, itching, and a sensation of warmth, with no increased risk in the elderly. 7,27 The safety and tolerability records extracted across our remotely supervised tDCS (RS-tDCS) randomized controlled trials (RCTs)10,28-30 showed that the side effects in a subsample of older participants (n=45, age range=65–78 years) with various neurological diseases (e.g., multiple sclerosis, Parkinson's disease, and cerebellar ataxia) did not differ in either nature or frequency from those in a subsample of young adults (old vs. young adults: tingling, 71% vs. 68%; itching, 35% vs. 41%; warmth sensation, 37% vs. 42%).

CLINICAL POTENTIAL OF tDCS IN AD

Notwithstanding the hundreds of clinical trials to date studying the clinical effects of tDCS, there remains the need for Class I/II evidence to advance its clinical use.² While the findings have largely been encouraging, most clinical trials have been limited by small samples and/or suboptimal dosing. As summarized in Table 1, several RCTs of tDCS have been conducted in AD or MCI over the last decade.

Dosing considerations

Preclinical model studies indicate that tDCS produces lasting changes in brain excitability (e.g., hemodynamic response, functional connectivity, and neuroplastic changes³¹⁻³⁴) that are cumulative over repeated sessions, which is consistent with clinical neurophysiology.^{23,35-38} Further, multiple-session protocols induce larger effects in terms of behavioral changes than do single-session protocols.³⁸⁻⁴²

Several studies have adopting 10 or fewer applications, which means that dosing may have been suboptimal for definitive evaluations of its clinical effectiveness. It is notable that recent studies involving relatively large numbers of total sessions over extended periods tended to show morerobust improvements in cognition with more-persistent effects, 38,43,44 relative to trials with smaller numbers of sessions over shorter periods. 42,45-48 This effect is mirrored through consistent findings across clinical studies, including in our own trials, showing that 1) a single tDCS session does not induce any meaningful behavioral response, 42 and 2) behav-

 Table 1. Summary of recent randomized controlled trials of tDCS in AD and MCI

Study	Participants	Active tDCS	Sham tDCS	Intensity, dose, and duration	Combination with another intervention	Assessment outcomes	Findings
Rasmussen et al. ⁸³	Mild-to-moderate AD (<i>n</i> =19: active=10; sham=9)	Anodal: left DLPFC	For 1 min, same montage	2-mA HD-tDCS for 20 min/session, 3 sessions/day for 2 days (total 6 sessions)	None	MMSE, clock-drawing test, TMT part A, RBANS, MRI including DTI	Short-term improvement in delayed-recall memory and global cognition. Positive correlation between FA in the anterior thalamic radiation with delayed memory score
He et al. ⁸²	MCI (n=43: active=24; sham=19)	Anodal: left DLPFC	For 1 min, same montage	1-mA HD-tDCS for 20 min/day, 5 sessions/week for 2 weeks (total 10 sessions)	None	MMSE, MoCA, resting-state fMRI	No improvement in cognition. Altered intensity and synchrony of brain activity in multiple regions on fMRI
Gangemi et al. ⁴³	Mild AD (<i>n</i> =26: active=13 and 9; sham=13 and 9)	Anodal: left frontotemporal	For 10 sec, same montage	Study 1: 2 mA for 20 min/day for 10 days (total 10 sessions) Study 2: 10 days/month for 8 months (total 80 sessions)	None	MMSE, MODA, EEG	Both short-term and long-term effects on the prevention of cognitive decline
Im et al. ³⁸	Mild AD (<i>n</i> =18: active=11; sham=7)	Anodal: left DLPFC Cathodal: right DLPFC	30-sec ramp up and 30-sec ramp down, same montage	2 mA for 30 min/day for 6 months (total 180 sessions)	None	MMSE, CDR and CDR-SOB, digit span, BNT, RCFT, SVLT, executive function tests, [18FJFDG PET	Long-term improvements in global cognition and language function. Marginally improved executive functions. Left middle/inferior temporal glucose metabolism was preserved on PET
Lu et al. ⁴⁴	MCI (<i>n</i> =201: active=69 and 68; sham=64)	Anodal: left lateral temporal cortex	For 30 sec, same montage	2 mA, 20 min/day, 3 sessions/week for 3 months (total 36 sessions)	WMT	N-back task, ADAS-Cog, MMSE, CDR-SOB, NPI, CVFT, digit span, logical memory, TMT	The combined tDCS-WMT group showed greater short-term improvements in delayed-recall and working memory, and long-term improvement in logical memory relative to single-modality groups
Gomes et al.™	MCI (<i>n</i> =58: active=29; sham=29)	Anodal: left DLPFC	For 30 sec, same montage	2 mA, 30 min/day, 2 sessions/week for 5 weeks (total 10 sessions)	None	CAMCOG, MMSE, TMT, semantic verbal fluency (animals), BNT, clock-drawing test, word-list memory, direct and indirect digit order, N-back task	Short-term improvement in memory recall, verbal fluency, and executive functioning



Table 1. Summary of recent randomized controlled trials of tDCS in AD and MCI (continued)

Study	Participants	Active tDCS	Sham tDCS	Intensity, dose, and duration	Combination with another intervention	Assessment outcomes	Findings
Khedr et al. ⁸⁰	Mild-to-moderate AD (<i>n</i> =46: active=23; sham=23)	Anodal: left and right temporoparietal	For 30 sec, same montage	2 mA, 20 min/day, 5 sessions/week for 2 weeks (total 10 sessions)	None	MMSE, MoCA, clock-drawing test, Cornell depression scale, serum tau, Aβ 1–42, lipid peroxidase	Short-term improvement in global cognition and depression, also correlated with increased plasma A β 1–42 levels.
Bystad et al. ⁴⁵	Bystad et al. 45 Mild-to-moderate Anodal: left AD (n=25: temporal active=12; Cathodal: rig sham=13) frontal	Anodal: left temporal Cathodal: right frontal	For 30 sec, same montage	2 mA, 30 min/day, 6 sessions in 10 days (total 6 sessions)	None	MMSE, CVLT, clock-drawing test, TMT, WAIS, Cornell depression scale	No significant improvement in cognition
Yun et al. ⁸¹	MCI (<i>n</i> =16: active=8; sham=8)	Anodal: left DLPFC Cathodal: right DLPFC	For 20 sec, same montage	2 mA, 20 min/day, 3 sessions/week for 3 weeks (total 9 sessions)	None	Modified MMQ, [¹8FJFDG PET	Short-term improvement of the memory strategies, increased regional cerebral metabolism on PET
Khedr et al. ⁸⁴	Mild-to-moderate Anodal: left AD (<i>n</i> =34: DLPFC active=11 and 12; Cathodal: left sham=11) DLPFC	Anodal: left DLPFC Cathodal: left DLPFC	For 30 sec, same montage	2 mA, 25 min/day, daily for 10 days (total 10 sessions)	None	MMSE, WAIS-III motor cortical excitability, P300 event-related potentials	Both anodal and cathodal tDCS improved short-term cognition and reduced the P300 latency
Cotelli et al. ⁴⁶	Mild-to-moderate Anodal: left AD (n=36: DLPFC active=12 and 12; sham=12)	Anodal: left DLPFC	For 20 sec at the beginning and end, same montage	2 mA, 25 min/day, 5 sessions/week for 2 weeks (total 10 sessions)	Individualized computerized memory training	FNAT, MMSE, ADL, IADL, Tinetti scale, NPI, Picture naming task, BADA, RBMT, Rey Auditory Verbal Learning Test, complex figure copying, TMT	No significant additive effect on the general improvement by memory training
Suemoto et al. ⁴⁷	Moderate AD (n=40: active=20; sham=20)	Anodal: left DLPFC	For 20 sec, same montage	2 mA, 20 min/day, 3 sessions/week for 2 weeks (total 6 sessions)	None s)	Apathy Scale, NPI, ADAS-Cog	No significant difference in apathy or cognition

AD, Alzheimer's disease; ADAS-Cog, Alzheimer's Disease Assessment Scale-Cognitive Subscale; ADL, activities of daily living; BADA, Battery for Analysis of Aphasic Deficits; BNT, Boston Naming Test; CAMCOG, Cambridge Cognition Examination; CDR, Clinical Dementia Rating; CDR-SOB, Clinical Dementia Rating-Sum of Boxes; CVFI, Category Verbal Fluency Test; DLPFC, dorsolateral prefrontal cortex; DTI, diffusion-tensor imaging; EEG, electroencephalography; FA, fractional anisotropy; fMRI, functional magnetic resonance imaging; FNAT, Face-Name Association Memory Task; HD, high definition; IADL, Instrumental Activities of Daily Living; MCI, mild cognitive impairment; MMQ, Multifactorial Memory Questionnaire; MMSE, Mini-Mental Status Examination; MoCA, Montreal Cognitive Assessment; MRI, magnetic resonance imaging; NPI, Neuropsychiatric Inventory; PET, positron-emission tomography; RBANS, Repeatable Battery for the Assessment of Neuropsychological Status; RBMT, Rivermead Behavioral Memory Test; RČFT, Rey Complex Figure Test; SVLT, Seoul Verbal Learning Test; tDCS, transcranial direct current stimulation; TMT, Trail-Making Test; WAIS, Wechsler Adult Intelligence Scale; WMT, working memory training.



ioral changes only follow a sustained period of daily treatment. 49,50 Multiple RCTs have shown that repeated application (i.e., \geq 20 daily sessions) of tDCS targeting the dorsolateral prefrontal cortex (DLPFC) improves cognitive training outcomes in healthy aging adults. 11,42,48 Importantly, these changes have also been linked to increases in the functional connectivity in the DLPFC 11 and in frontal lobe neurotransmitter concentrations. 51

In previous trials there have also been wide variations in the dosing parameters applied to the electrode montage (functional targeting vs. lesion-based targeting), electrical current intensity, stimulation duration, and the number of applied stimuli, as well as in the application of simultaneously paired training activities across study designs. Four of the 12 RCTs listed in Table 1 involved MCI patients, and the remainder involved patients with mild or moderate AD. Almost all of these studies used anodal tDCS (i.e., with the anode electrode over the target region) with a current of 2 mA for 20-30 min per session. The nominal target region varied, although the most-common target region was the DLPFC (left>right), F3-F4 according to the international 10-20 system), while temporal targeting has been applied less, hence warranting further studies. The total number of sessions varied markedly between 6 and 180, with the overall treatment duration varying between 2 days and 8 months.

We now know that neuroplasticity can occur throughout the lifespan, and the neuroplastic effects induced by tDCS have been demonstrated to be preserved in healthy elderly individuals. ⁵¹⁻⁵⁴ However, critical guidance concerning tDCS dosing parameters is needed in order to maximize its clinical benefit in the presence of neurophysiological age-related changes; ⁵⁵ for example, age may affect the optimal current intensity ^{27,56-58} and stimulation duration. ⁵⁹ Further, various factors such as the brain state, brain atrophy, and hormonal levels are likely to influence individual differences in response, and so they can ultimately be used to identify those who are most likely to benefit from treatment. ^{6,27,60,61}

Simultaneous pairing of tDCS with cognitive training

tDCS can target the neuromodulation of regions underlying cognitive impairments or be paired with simultaneous cognitive training. When paired together with training tasks, the targeted region (functional targeting) is engaged both through the stimulation and simultaneous activity, which may produce a synergistic benefit. In MCI and AD, investigators have taken approaches to employ neuromodulation with tDCS with the goal of both improving cognitive functioning and ultimately delaying or even preventing its progressive decline. Studies have targeted stimulation of frontal or tem-

poral regions, often pairing with simultaneous cognitive training exercises. 44,46 This approach activates the target region by the activity during the stimulation, and may lead to improved cognitive training outcomes.

Only two RCTs have used cognitive training as an intervention combined with tDCS (see Table 1)-such a combined intervention may be especially effective in potentiating and strengthening the learning process. 62 The simultaneous delivery of tDCS with cognitive training is broadly thought to increase potential neuronal firing and synaptic activity, which will selectively activate and reinforce the regions engaged in the cognitive activity, 63-65 with these positive effects being transferred to similar tasks.⁶⁶⁻⁶⁹ The findings of recent electrophysiological studies analyzing the mechanism of tDCS suggest that the long-term effects of tDCS are due to the enhancement of neural plasticity by modulating longterm potentiation and depression in relevant neural networks. 20,65 This combined approach may have the added benefit of prolonging learning effects after the treatment has ceased.70-73 As demonstrated by our previous work across neurodegenerative disorders, pairing DLPFC tDCS with cognitive training increases learning and performance outcomes, and leads specifically to improvements in measures of vigilance. 10,12,74-78

Long-term efficacy

No previous study has addressed the important question of the persistence of benefits. Due to the small number of trials with follow-ups longer than 1 month, further studies are needed to determine whether the established effects of tDCS persist over time once treatment has been discontinued. This question is critical when considering the potential of tDCS in preventing or delaying cognitive decline in MCI and AD patients over time.⁷⁹

THE NEED FOR MECHANISTIC INSIGHT

For the outcome measurements of the latest RCTs in Table 1, basic and global cognitive assessment tools such as the Mini-Mental Status Examination, Montreal Cognitive Assessment, and Clinical Dementia Rating were used the most, with most studies also including more-comprehensive measures for specific domains. Only one of the studies that evaluated psychiatric symptoms found a significant improvement in depression.⁸⁰

However, only a handful of studies have used neuroimaging or electrophysiological methods as secondary outcomes. Im et al.³⁸ and Yun et al.⁸¹ used [¹⁸F]FDG positron emission tomography (PET) to visualize changes in the cerebral glu-



cose metabolism after tDCS, and both studies found significant positive effects. Recent studies using resting-state functional magnetic resonance imaging or diffusion tensor imaging have also demonstrated the utility of advanced neuroimaging tools for assessing the outcome of tDCS. $^{82.83}$ Khedr et al. 84 measured motor cortical excitability using TMS and P300 latency in event-related potentials at baseline and after tDCS sessions. In a subsequent study they measured the following blood markers for AD at baseline and after tDCS: tau, A β 1–42, and lipid peroxidase. 80 Thus, promising findings from the small number of trials using multimodal outcome measures warrant further studies taking advantage of the rapid advances in technology in clinical neuroscience in order to understand the complex therapeutic mechanisms of tDCS.

Various neurotransmitters have been suggested to be involved in the mechanisms of the changes resulting from tDCS applications, including dopamine, acetylcholine, serotonin, glutamate, and GABA.85 For example, a PET investigation with [11C]raclopride demonstrated that applying a single session of tDCS to the DLPFC induced dopamine release in the ventral striatum, which was associated with attention enhancement in healthy humans. 86 Likewise, there is good evidence from both animal and human studies for the strong involvement of the serotonin system in the antidepressant effect of tDCS on the DLPFC.87,88 More importantly for AD, there are accumulating data suggesting the pivotal role of the cholinergic neurons and their synaptic modulation in the changes induced by tDCS. 85,89,90 Neurophysiological studies in animals have shown that cholinergic modulation facilitates long-term potentiation. 91,92 Previous human studies of tDCS combined with an acetylcholinesterase inhibitor or nicotine patch also demonstrated the significant contribution of the cholinergic pharmacodynamic status on the different levels of neuroplasticity induced by tDCS. 93,94 In addition, recent tDCS investigations involving MCI and AD patients demonstrated significant increases in cortical metabolism in the areas relevant to cholinergic synaptic innervation, such as the prefrontal, anterior cingulate, and medial and lateral temporal cortices.^{38,81} A recent study utilizing magnetic resonance spectroscopy demonstrated increased GABA and a decreased ratio of glutamate to GABA after tDCS in older adults with or without MCI.95 To our knowledge, that is the only previous clinical trial of tDCS in AD or MCI that has employed outcome measures that can detect specific changes in each of those neurotransmitters, which should be seriously considered when planning future studies.

HOME-BASED tDCS USING REMOTE SUPERVISION IN DESIGNING CLINICAL TRIALS

Both tDCS and cognitive training must be dosed in a sustained and cumulative manner to induce an effect. However, as detailed above, previous trials of tDCS and cognitive training in AD or MCI have only allowed restricted conclusions to be drawn, ⁹⁶ due in part to the potential underdosing in terms of the frequency and number of treatment sessions being lower than those required for an optimal effect. ⁹⁷⁻⁹⁹

We believe that trial designs have been restricted by practical obstacles associated with accessing treatment in the clinic. The logistical constraints of clinic-based treatment such as participant time and travel as well as costs for daily visits—have been a primary and practical limitation for the field in terms of sample size and suboptimal dosing of the number of sessions. To enhance access to treatment and enable protocols with extended treatment periods, we have validated an RS-tDCS protocol that delivers treatment at home to as to overcome practical barriers to access and thereby facilitate cumulative dosing. There has been a strong demand for such at-home treatment across various neurological conditions, including for people with multiple sclerosis, Parkinson's disease, traumatic brain injury, and cerebellar ataxia, which have led to clinical applications. 10,13,14,28-30,100-104 In the RS-tDCS protocol, participants are provided with remotely controlled tDCS devices, and they are extensively trained in their safe and effective operation. We apply real-time supervision in each tDCS session through live videoconferencing with extensively trained personnel who follow rigorous go/ no-go criteria during the daily treatments in order to ensure that the protocol complies with the laboratory standards of the tDCS devices. 13,100,105

The telehealth delivery of tDCS results in rapid enrollment and high retention and adherence rates in repeated and extended sessions (e.g., >97% completion rates across RCTs to date). 10,13,14,28-30,100-104 Extensive testing over >7 years (covering >9,000 at-home tDCS sessions involving >400 patients to date) has verified the feasibility of our RS-tDCS procedures for use across all ages (18-80 years), including in those with advanced cognitive or motor disabilities and/or low technical experience, and it also reaches those whose poor socioeconomic healthcare status impedes their inclusion in RCTs. Further, the RS-tDCS platform has facilitated continuing enrollments in ongoing RCTs during the restrictions to clinical research associated with the COVID-19 pandemic, with >100 participants completing all study procedures from home. 106-109 Only one previous study evaluated tDCS in the home setting, by providing unsupervised tDCS to pa-



tients with mild AD over 6 months and without concurrent cognitive training activity.³⁸ That study confirmed the safety and feasibility of the home use of tDCS in the AD population, and also demonstrated the mild general cognitive improvements achieved, indicating that remotely supervised home-based trials can facilitate the design of further clinical trials.38

CONCLUSIONS AND FUTURE DIRECTIONS

Further investigations are needed into the efficacy of tDCS and cognitive training with sufficient dosing over longer follow-ups. The inclusion of biomarkers for guidance is critical to advancing the field and developing new therapeutic targets. With the goal of delaying progression, the MCI population represents the earliest and best target group for further evaluation. The effects on neuroplasticity in MCI can be investigated by including a sensitive biomarker of the underlying mechanism. Finally, the additive effects of the combined intervention of tDCS and cognitive training have not been thoroughly evaluated relative to applying tDCS and cognitive training separately in a study design with adequate intensity, duration, and scientific rigor.

Future clinical trials of tDCS in AD and MCI need to be performed under optimized conditions based on the accumulating evidence for the importance of a longer follow-up. Namely, a sufficient number of sessions over an extended period should be administered in conjunction with cognitive training. Outcomes should be assessed using a multimodal approach that includes neuroimaging, electrophysiological, or other AD-specific biomarkers in combination with conventional neuropsychological testing. In order to gain a better understanding of the mechanism so as to guide AD treatments, further studies employing a specific biomarker that can sensitively detect modulation of the targeted neural system are necessary. We propose that home-based RS-tDCS is a practical solution for promoting the clinical use of tDCS by the MCI and AD population. The next investigative steps could lead to tDCS and other noninvasive brain stimulation approaches representing an important clinical tool for the care of AD patients.

Availability of Data and Material

Data sharing not applicable to this article as no datasets were generated or analyzed during the study.

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Conflicts of Interest

Min-Jeong Kim, a contributing editor of the Journal of Clinical Neurology, was not involved in the editorial evaluation or decision to publish this article.

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